



Europäisches Patentamt

European Patent Office

Office européen des brevets



(11)

**EP 0 812 571 A1**

(12)

## EUROPEAN PATENT APPLICATION

(43) Date of publication:  
17.12.1997 Bulletin 1997/51

(51) Int. Cl.<sup>6</sup>: **A61B 17/00**, A61B 17/04

(21) Application number: **97301486.3**

(22) Date of filing: **05.03.1997**

(84) Designated Contracting States:  
**DE ES FR GB IT NL**

(30) Priority: **11.06.1996 US 661844**

(71) Applicant: **Cardiologics, L.L.C.**  
**Totowa, New Jersey 07512 (US)**

(72) Inventor: **Kontos, Stavros**  
**Woodcliff Lake, New Jersey 07675 (US)**

(74) Representative:  
**Bayliss, Geoffrey Cyril et al**  
**BOULT WADE TENNANT,**  
**27 Furnival Street**  
**London EC4A 1PQ (GB)**

### (54) Device for suturing blood vessels and the like

(57) A method and device (1) for sealing an opening in an anatomical structure within a living body involves the positioning of the tissue adjacent to the opening within a gap between proximal and distal parts (18,24) of a flexible tube (16) formed by a curved central part (22). A needle (37) coupled to a suture loop (41) is drawn from a needle retention channel (32) formed within the distal part (24) through the tissue received in the gap and into a needle receiving channel formed within the proximal part (18). The needle (37) may be

drawn out by pulling on either the suture loop (41) or a separate pull cord (43) which extends through a lumen to an opening formed in the first end of the proximal part (18). After the device (1) has been rotated and the procedure repeated, a second needle (37) attached to the suture loop (41) is drawn through the tissue in the same manner and the two ends are knotted together and tightened to seal the opening.

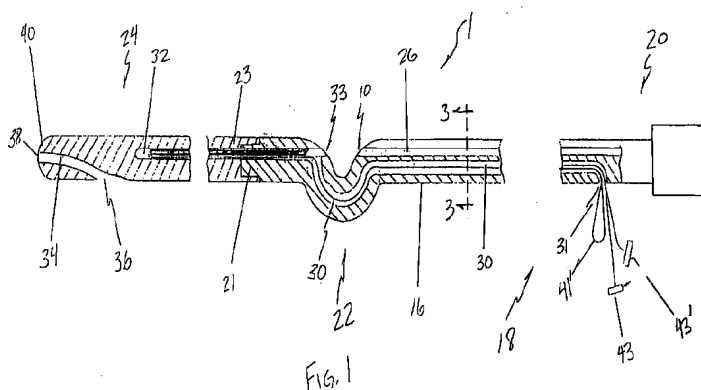


Fig. 1

EP 0 812 571 A1

## Description

The present invention relates generally to surgical instruments, and more specifically to devices for the suturing of punctures in blood vessels, internal organs and internal tissues accessed via a tissue tract.

Many surgical procedures require the insertion of catheters and/or surgical devices into blood vessels and other internal structures. For example, in the treatment of vascular disease, it is often necessary to insert an instrument, i.e., a catheter, into the blood vessel to perform the treatment procedure. Such treatment procedures often involve piercing a wall of the blood vessel, inserting an introducer sheath into the blood vessel via the opening, and maneuvering the procedural catheter through the introducer sheath to a target location within the blood vessel. Of course in order to complete such a procedure, the sides of the opening in the wall of the blood vessel must be sealed to prevent bleeding while facilitating healing of the wound. At present, this sealing is commonly accomplished by application of direct pressure over the puncture site by a physician or other trained medical professional. Due to the dangers of thrombosis, the substantial reduction of blood flow through the blood vessel due to the application of pressure is undesirable and potentially dangerous to the patient. In addition, the procedure is extremely time consuming; often requiring that pressure be applied for forty-five minutes or more to achieve acceptable sealing.

Other sealing techniques include the application of a biogenic sealing material over the opening to seal the wound. However, proper placement of the sealing material is difficult to achieve and, the plug of sealing material left inside the blood vessel may result in serious health risks to the patient.

As a result, devices have been developed which are inserted through the puncture in order to suture openings created in blood vessels. However, these devices suffer from various drawbacks.

For example, U.S. Patent No. 5,417,699 to Klein et al. describes a device wherein two needles coupled to a distal end of an insertion shaft are surrounded by an outer sheath during insertion into an internal structure. Once inside the internal structure, the outer sheath is withdrawn and bowed sections of the needles, which had been constrained within the outer sheath against an outward spring bias, deploy away from the insertion shaft. The insertion shaft is then withdrawn drawing the needles through the walls of the internal structure. The arcuate shape of the needles is intended to bring the needles back along a curved path toward the insertion shaft so that the free ends of the needles may be captured on the shaft and the device withdrawn from the body. Thereafter, the distal ends of the needles must be detached from the insertion shaft so that a length of suture extending between distal ends of the two needles may be drawn through the walls of the internal structure to seal the opening.

However, the curved shape of the proximal ends of the needles of this device requires an insertion sheath of increased diameter. Thus, after withdrawal of a treatment catheter from an opening formed in an internal structure, insertion of the increased diameter outer sheath of the device of Klein et al. actually expands the opening in the wall of the internal structure. In addition, the device of Klein et al. employs several slidably mounted concentric shafts and mechanisms for the deployment and capture of the needles which make the device costly to manufacture and cumbersome to operate.

The present invention is directed to a device for sealing an opening in an anatomical structure within a living body. The device includes a flexible tube including a proximal portion extending along an axis coupled to a distal portion extending along the axis by a central portion, wherein the central portion extends away from the axis to form a gap between a distal end of the proximal portion and a proximal end of the distal portion. A needle retention channel formed within the distal portion for holding a plurality of needles therein extends along the axis to an opening formed in the proximal end of the distal portion. In addition, a needle receiving channel formed within the proximal portion extends along the axis to an opening formed in the distal end of the proximal portion. Finally, a lumen extends from an opening formed in the end of the proximal portion to the needle retention channel. Thus, when the device is in an operative position, the flexible tube extends through the opening in the anatomical structure with the opening in the distal end of the proximal portion and the opening in the proximal portion on opposite sides of the anatomical structure.

The present invention is also directed to a method including the steps of guiding into an opening in an anatomical structure, a device including a substantially linear proximal and distal portions extending along a common axis and a curved central portion coupling the proximal and distal portions so that a gap is formed therebetween. The device is positioned so that the curved central portion is within the opening with a needle retention channel opening on a distal side of the anatomical structure and a needle receiving channel opening on a proximal side of the anatomical structure. The doctor then draws a pull cord attached to a distal end of a first needle out to bring a first needle proximally out of the needle retention channel through the anatomical structure and through the needle receiving channel to bring a first end of the suture through the anatomical structure. Thereafter, the device is rotated to a second desired position so that a second portion of the anatomical structure adjacent to the opening is located within the gap and a pull cord attached to a distal end of a second needle is drawn to bring the second needle proximally out of the needle retention channel through the anatomical structure and into the needle receiving channel so that the second end of the suture is drawn through the anatomical structure. The first and second ends of the

suture are then secured together to seal the opening.

A further embodiment of the invention is directed to a surgical stitching device comprising a flexible tube including substantially linear proximal and distal portions defining an axis and a curved central portion coupling the proximal and distal portions so that a gap is formed therebetween. A puncture needle channel extends through the proximal portion along the axis to an opening formed in the distal end of the proximal portion, while a puncture needle receiving channel extends through the distal portion along the axis to a suture retention channel of relatively larger cross-sectional area. A puncture needle including a central lumen is slidably received in the puncture needle channel so that, by applying pressure to a proximal end of the puncture needle, a user may manually move the puncture needle out of the opening formed in the distal end of the puncture needle channel, across the gap and into the puncture needle retention channel until a distal end of the puncture needle is received within the suture retention chamber. A piston is slidably received in the central lumen so that, when the distal end of the puncture needle is received within the suture retention chamber, a user may move the piston distally through the central lumen to release the contents of the central lumen into the suture retention chamber.

The invention will now be described in detail, by way of example only, with reference to the accompanying drawing, in which:

Figure 1 shows a side view of a cross-section of a suturing device according to a first embodiment of the invention;

Figure 2 shows a top view of a cross-section of a suturing device according to the first embodiment of the invention;

Figure 3A shows a cross-section of a device according to the first embodiment of the invention taken along line 3-3 of Fig. 1;

Figure 3B shows an alternative cross-section of a device according to the first embodiment of the invention taken along line 3-3 of Fig. 1;

Figure 4A shows a cross-section of a device according to the first embodiment of the invention taken along line 4-4 of Fig. 2;

Figure 4B shows an alternative cross-section of a device according to the first embodiment of the invention taken along line 4-4 of Fig. 2;

Figure 5 shows a partially cross-sectional view of a blood vessel within a body with a guide wire inserted therein;

Figure 6A shows a partially cross-sectional view of the blood vessel with a device according to the first embodiment of the present invention received on the guide wire in a first desired position;

Figure 6B shows a partially cross-sectional view of the blood vessel with the device as shown in Fig. 6A wherein a needle has been drawn through the body tissue received in the central gap;

Figure 7 shows a partially cross-sectional view of the blood vessel with a device according to the first embodiment of the present invention in a second desired position;

Figure 8 shows a partially cross-sectional view of the blood vessel with a device according to the first embodiment of the present invention partially removed from the blood vessel;

Figure 9 shows a slip knot tied in a suture loop extending through the wall of the blood vessel being urged toward the blood vessel;

Figure 10 shows a suture sealing the puncture;

Figure 11 shows a side view of a cross-section of a suturing device according to a second embodiment of the invention;

Figure 12 shows a cross-section of a device according to the second embodiment of the invention taken along line 12-12 of Fig. 11;

Figure 13 shows a cross-sectional view of a puncture needle according to the second embodiment of the present invention;

Figure 14 shows a side view of a plunger according to the second embodiment of the present invention;

Figure 15 shows a partially cross-sectional view of the blood vessel with a device according to the second embodiment of the present invention in a first desired position;

Figure 16 shows a partially cross-sectional view of the blood vessel with a device according to the second embodiment of the present invention in the first desired position where a suture has been passed through the wall of the blood vessel and introduced into a suture retention chamber;

Figure 17 shows a partially cross-sectional view of the blood vessel with a device according to the second embodiment of the present invention in a second desired position;

Figure 18 shows a partially cross-sectional view of the blood vessel wherein the device according to the second embodiment has been partially withdrawn from the blood vessel;

Figure 19 shows a partially cross-sectional view of the blood vessel wherein the sutures have been severed from the anchor members and tied together;

Figure 20 shows a side view of a cross-section of a distal portion of a suturing device according to a third embodiment of the present invention; and

Figure 21 shows a cross-section of a distal portion of a device according to the fourth embodiment of the invention.

Referring now to the drawings, in which like reference numerals identify similar or identical elements, Figs. 1 - 8 show a device 1 according to a first embodiment of the invention for suturing punctures in blood vessels, internal organs and the like. The device 1 includes flexible tube 16 of substantially circular cross-section, which has a proximal part 18 and a distal part

24. The proximal part 18 extends from a first end 20 through a central arcuate portion 22 to a second end 21 which mates with a proximal end 23 of the distal part 24. The central arcuate portion may preferably be substantially circular with a radius of from 0.100" to 0.600". The flexible tube 16 is preferably constructed of a thermoplastic such as polyurethane, polyethylene, or the like, in two or three parts bonded together. The various parts of the flexible tube 16 may preferably be either extruded or molded. Those skilled in the art will recognize that it will be more economical to extrude the parts including one or two lumens, while the more complex, and curved sections of the flexible tube 16 may be molded. The length of the flexible tube may be selected to fit the requirements of a particular situation and is preferably between 1" and 16" in length.

The flexible tube 16 includes a large interior needle withdrawal lumen 26 which extends through the proximal part 18 from the first end 20 to an opening 10 at a proximal end of the central arcuate portion 22. As seen in Figs. 3A and 3B, the needle withdrawal lumen 26 may preferably be oval in cross-section and may include an optional slot 28 opening to the outside of the flexible tube 16.

In addition, a flash back lumen 30 extends from an opening 31 formed in the proximal part 18 through the central arcuate portion 22 to open into two needle retention bores 32 and 32' formed side-by-side in the distal part 24. As seen in Fig. 3A, the flash back lumen 30 may be circular in cross-section and is sized to simultaneously accommodate two strands of the suture 41 and the two pull cords 43 and 43'. However, as shown in Fig. 3B, the cross-section of the flash back lumen 30 may preferably include side-by-side hemispherical channels 45 and 45' for receiving the loop 41' of the suture 41 and the two pull cords 43 and 43'. This helps to ensure that the second needle 37 is not accidentally drawn out of the needle retention bore 32' when the first 37 is being pulled out. The needle retention bores 32 and 32' extend from distal ends to openings 33 and 33', respectively, formed at a position in the distal end of the central arcuate portion 22 opposite the opening 10. In addition, a substantially straight stiffening member may be inserted into the flash back lumen 30 in order to straighten the central arcuate portion 22 during insertion of the device 1 into the body. Alternatively, the device 1 may be made straight and, after insertion into the body, a curved stiffening member may be inserted to bend the device 1 thereby creating the central arcuate portion 22.

As seen in Figs. 4A and 4B, the retention bores 32 and 32' have cross-sectional shapes including first portions 35, each shaped to receive a needle 37 and second portions 39, each shaped to receive a suture 41 and pull cord 43 or 43'. The first portions 35 are shaped to correspond to the cross-section of the needles 37 which in the preferred embodiment is substantially circular. The second portions 39, which are of reduced size so that the needles 37 are unable to enter, may be

either rectangular or triangular projections extending from the first portions 35 and are sufficiently large to simultaneously accommodate the suture 41 and one of the pull cords 43 and 43'. The suture 41, which will preferably be in the range of 0.004" to 0.010" in diameter and from 15" to 35" in length, may be formed of either "reabsorbable" or "non-reabsorbable" material, as is well known in the art. The pull cords 43 and 43' will preferably be formed of non-reabsorbable material and will be of similar diameter to the suture 41. Those skilled in the art will recognize that the function of the pull cords 43 and 43' may be filled by a loop 41' of the suture 41 coupled between the distal ends of the needles 37 extended through the flash back lumen 30 so that, when the loop 41' of the suture 41 is extended proximally, the needles 37 are urged proximally through the needle retention bores 32 and 32'.

As the device 1 according to the first embodiment includes a single pair of needles, this device should preferably be used to close punctures of 9.0 French size and smaller (each French size representing 0.13" in diameter). The flexible tube 16 will, therefore, preferably be 6.0 or 8.0 French size. As described below in reference to further embodiments of the invention, devices employing two or more pairs of needles 37 may be employed to close punctures larger than 9.0 French size. Each of the needles 37 may preferably be constructed of stainless steel, be between 2" and 8" in length and have a diameter between 0.010" and 0.030".

When the device 1 is in an operative configuration, the suture 41 extends between the distal ends of two needles 37 received in the needle retention bores 32 and 32'. In the first embodiment of the invention, optional pull cords 43, 43' extend from the distal end of each of the needles 37 through the second portions 39 of the needle retention bores 32 and 32', via the flash back lumen 30, to the opening 31. However, the suture 41 may, alternatively, extend from the distal ends of the needles 37 through the second portions 39 of the needle retention bores 32 and 32', via the flash back lumen 30, to the opening 31 so that a portion of the suture loop 41' which extends out from the opening 31 may provide the function of the pull cords 43 and 43', as described below.

Finally, a guide wire lumen 34 extends through the distal part 24 of the device 1 from a proximal opening 36 to a distal opening 38 formed in a second end 40 of the device 1.

In operation, as shown in Figs. 5 - 10, when an invasive procedure is performed on a patient which requires the insertion of a catheter into a blood vessel (or other structure within the body), an introducer sheath is inserted through the skin (S) into the patient's body through a puncture (P) in a wall of the blood vessel (BV). A guide wire 44 is inserted through the puncture to a target area within the blood vessel and a catheter is inserted through the introducer sheath, along the guide wire 44, to a target area within the blood vessel. After the procedure is complete, the catheter and the intro-

ducer sheath are withdrawn and the guide wire 44 is left in place. A proximal end of the guide wire 44 is then inserted through the guide wire lumen 34 and the device 1 is inserted into the body and moved along the guide wire 44 through the puncture until the central arcuate portion 22 straddles a portion of the blood vessel wall adjacent to the puncture.

By observing the flash back lumen 30 and the needle withdrawal lumen 26, the doctor may determine when the device 1 is in the desired position. Specifically, when the device 1 is inserted far enough into the blood vessel, blood will be observed in the flash back lumen 30. However, if blood is observed in the needle withdrawal lumen 26, the doctor knows that the device 1 has been inserted too far into the blood vessel.

As the device 1 is inserted into the blood vessel, the flexible tube 16 bends so that the device 1 is received within, and extends in the direction of the blood vessel without straining the vessel. In this position, the openings 33 and 33' are on the distal side of the puncture facing the opening 10 which is located on the proximal side of the puncture.

As shown in Fig. 6B, the doctor then rotates the device 1 into a desired orientation and draws the pull cord 43 out of the opening 31, thus drawing one of the needles 37 forward through the needle retention bore 32 so that a pointed, proximal end of the needle 37 is drawn through the wall of the blood vessel, enters the opening 10 and extends into the needle withdrawal lumen 26. The needle 37 is then withdrawn through the needle withdrawal lumen 26, drawing a first end of the suture 41 through the wall of the blood vessel and into the needle withdrawal lumen 26. The needle 37 is drawn forward by means of the pull cord 43 until a proximal end of the needle 37 protrudes from the proximal end of the needle withdrawal lumen 26. The proximal end of the needle 37 is then grasped by the doctor and withdrawn from the needle withdrawal lumen 26. In order to ensure that the needles 37 will extend through the needle withdrawal lumen 26, the needles 37 will preferably be at least 4" in length.

Thereafter, the doctor rotates the device 1, as shown in Fig. 7, until the central arcuate portion 22 straddles the blood vessel wall in a desired position relative to the point at which the first end of the suture 41 penetrated the blood vessel wall. Those skilled in the art will understand that this "desired position" will usually be on the opposite side of the puncture, so that the device 1 will be rotated approximately 180° after the first needle 37 is withdrawn. When the device 1 is in the second desired orientation, the doctor draws the pull cord 43' out of the opening 31 thereby urging the second needle 37 forward through the needle retention bore 32' so that the pointed, proximal end of the second needle 37 is drawn through the wall of the blood vessel, enters the opening 10 and extends into the needle withdrawal lumen 26. The second needle 37 is withdrawn through the needle withdrawal lumen 26, drawing the second end of the suture 41 through the wall of the blood vessel

and into the needle withdrawal lumen 26 as described above.

As shown in Figs. 8 - 10, the doctor withdraws the device 1 from the body and detaches the suture 41 from the ends of the needles 37 and ties the two ends together in a slip knot which is urged inward toward the blood vessel and drawn tight in order to seal the puncture. Of course, those skilled in the art will appreciate that, once the two ends of the suture 41 have been drawn through the blood vessel wall, various other methods of fastening the two ends together may be employed.

Figs. 11 - 19 show a suturing device according to a second embodiment of the present invention. The flexible tube 16 of the device 1' according to the second embodiment is preferably similar in size and flexibility to the device 1 of the first embodiment and differs only as described below. In addition, those skilled in the art will recognize that, except where specifically stated, each of the variations described above in reference to the first embodiment may also be applied to all other embodiments.

As seen in Fig. 12, the cross-section of the proximal part 18 of the device 1' shows a flash back lumen 30 of circular cross-section. The flash back lumen 30 of this embodiment extends from the first end 20, through the proximal part 18 to an opening 49 formed adjacent to the opening 68.

In addition, instead of the needle withdrawal lumen 26 of the first embodiment, the proximal part 18 of the device 1' includes a substantially circular-puncture needle channel 50 extending from the first end 20 of the device 1' to an opening 52 at a proximal end of the central arcuate portion 22. This puncture needle channel 50 is also shown including an optional slot 54 extending through the surface of the flexible tube 16 along the length of the puncture needle channel 50.

A puncture needle 56, having an increased diameter gripping surface 58 at a proximal end, is slidably received in the puncture needle channel 50. The puncture needle 56 includes a central channel 59 extending from an opening 60 formed in the gripping surface 58 to an opening 61 formed in a distal end 62 of the puncture needle 50. One suture 41, integrally formed with or coupled to a respective anchor member 64, is received within the central channel 59. The anchor member 64 may be constructed as a coiled stainless steel spring.

Those skilled in the art will recognize that, if the puncture needle 56 is provided with a slot extending from a proximal end to a distal end thereof, a suture loop 41' may be formed with a single suture 41 having anchor members 64 at both ends. That is, after a first end of the suture has been inserted into the suture retention chamber 72, a first length of this suture 41 may be drawn out through the slot and a second anchor member 64 attached to a second end of the suture 41 may be inserted into the suture retention chamber 72 through a second portion of the blood vessel wall as described above. Thereafter, the device 1' is withdrawn

from the body and the two ends of the suture loop 41' are tied together and, using known techniques, the knot is maneuvered so that it ends up on the outside of the blood vessel.

A plunger 66 is slidably received within the central channel 59 so that the anchor member 64 is located between the opening 61 and a distal end of the plunger 66 so that, when the plunger 66 is urged distally into the central channel 59, the anchor member 64 is moved toward the opening 61.

An opening 68 opposite the opening 52 at a distal end of the central arcuate portion 22, extends through a needle reception slot 70 to a suture retention chamber 72 which has an increased diameter relative to the needle reception slot 70. Those skilled in the art will recognize that many variations may be made to the structure of the anchor member 64 so long as sufficient stiffness is maintained and the anchor member is dimensioned so as to prevent the suture 41 from being withdrawn from the suture retention chamber 72 during withdrawal of the device 1' from the body.

In operation as shown in Figs. 15 - 19, the device 1' is positioned with the central arcuate portion 22 straddling the blood vessel wall with the openings 52 and 68 on opposite sides of the wall (proximal and distal, respectively) and rotated to a desired position as described above in regard to the device 1 of the first embodiment.

As described above in regard to the device 1, the flash back lumen 30 may be used to determine whether or not the device 1' is in the desired position. Specifically, when the device 1' is in the desired position, blood should be observed only in the flash back lumen 30, not in the needle channel 50. Blood in the needle channel 50 indicates that the device 1' has been advanced too far into the blood vessel. That is, blood in the needle channel 50 indicates that the opening 52 is improperly positioned within the blood vessel. When the device 1' is properly positioned, the doctor presses upon the gripping surface 58 to urge the a sharp, distal end of the puncture needle 56 distally out of the opening 52, through the wall of the blood vessel and into the opening 56.

When the puncture needle 56 has been inserted into the suture retention chamber 72, the doctor pushes the plunger 66 distally within the central channel 59 to release the anchor member 64 into the suture retention chamber 72. The puncture needle 56 is then withdrawn from the suture retention chamber 72 and the plunger 66 is completely withdrawn from the central channel 59.

Where the device 1' includes the optional slot 54, the suture 41 may then be withdrawn from the puncture needle channel 50 through the slot 54. This allows the diameter of the puncture needle channel 50 to be minimized while providing sufficient room for the puncture needle 56 to pass therethrough. Then a second anchor member 64 and a second suture 41 are inserted into the central channel 59.

As shown in Fig. 17, the doctor then reorients the

device 1' into the second desired position, as described above in regard to the first embodiment, the doctor presses upon gripping the surface 58 to urge the sharp, distal end of the puncture needle 56 distally out of the opening 52, through the wall of the blood vessel and into the opening 56 so that the opening 61 is within the suture retention chamber 72. Thereafter, the doctor inserts the plunger 66 into the central channel 59 and pushes it forward to release the anchor member 64 and the second suture 41 into the suture retention chamber 72. Those skilled in the art will understand that, instead of inserting a second suture 41 at this point, a gripping device may be introduced through the central channel 59 into the suture retention chamber 72 to grab and retrieve the anchor member 64 and draw it out through the central channel 59. This allows for the formation of a suture loop 41' without the need to knot two separate strands of suture 41 together.

The doctor then withdraws the device 1' from the body, as shown in Fig. 22, so that the ends of the sutures 41 extending from the opening 68 may be cut to release the sutures from the anchor members 64. Then, as shown in Figs. 23 and 24, these ends of the sutures 41 are tied together and the other ends are knotted together and tightened to seal the puncture.

Those skilled in the art will understand that, for larger punctures, the device 1" may be used to insert as many sutures 41 as are required to seal the puncture. Specifically, in order to close punctures larger than size 9.0 French, a single suture 41 may not be sufficient. Therefore, instead of using the device 1" as described above to insert two sutures 41 approximately 180° apart, a doctor may, for example, insert four sutures 41 at 90° intervals using the technique described above. Then, when the device 1" has been withdrawn from the body, the doctor must knot together a first pair of sutures 41 which are separated by approximately 180° and then knot the second pair. The two pairs of sutures 41 may be distinguished by color coding or any similar technique.

A device 1" according to a third embodiment of the present invention is shown in Figs. 25 and 26. Aside from a modified distal part 24 as described below, the construction and operation of the device 1" may be identical to either of the first and second embodiments.

Specifically, the distal part 24 of the device 1" is constructed so that it has enhanced flexibility relative to the proximal part 18. In addition, the distal part 24 is biased so that, when in an unstressed state, it is "J" shaped - that is, the distal part 24 is curved so that the distal opening 38 formed in the second end 40 faces proximally. This facilitates insertion of the device 1" so that it contacts an inner wall of the blood vessel without damaging it. Specifically, the flexibility and "J" shape of the second end 40 allows the second end 40 to deflect away from the blood vessel's lining without penetrating or damaging the lining thereof. Of course, when received on the guide wire 44, the "J" shape of the distal part 24 will be less pronounced. However, the bias will

maintain a slight curvature of the second end 40 deflecting the impact of the device 1" from the inside lining of the blood vessel.

As described above, in order to close punctures larger than size 9.0 French, a single suture 41 may not be sufficient. Thus, as shown in Fig. 21, a device 1" according to a fourth embodiment of the invention may receive four needles 37 arranged side-by-side in four needle retention bores 32 formed in a flexible tube 16 of substantially oval cross-section. Other than the oval cross-section and the provision of four needles, the construction and operation of the device 1" is similar to that of the device 1 according to the first embodiment.

The oval cross section increases the stiffness of the device 1" in the plane in which the four needles lie side-by-side, while retaining flexibility to bend perpendicularly to that plane. The four needles 37 of the device 1" are coupled together in pairs and each pair of needles will be positioned so that the needles 37 of each pair penetrate the wall of the blood vessel on opposite sides of the puncture (approximately 180° apart). When the device 1" has been removed from the body, each pair is then knotted together and the two knots are tightened to seal the puncture.

Of course, those skilled in the art will understand that each of the variations of the device 1 according to the first embodiment may also be applied to the device 1". Similarly, those skilled in the art will recognize that four needles 37 may be received in a device 1" having two needle retention bores 32, each being of a length sufficient to hold two needles 37 arranged in series end-to-end.

There are many variations of the above described embodiments which will be apparent to those skilled in the art. It is understood that these modifications are within the teaching of the present invention which is to be limited only by the claims appended hereto. In addition, although the operation of the various embodiments has been described in regard to the sealing of an opening in the wall of a blood vessel, those skilled in the art will understand that this invention may also be used to seal openings in various internal organs and structures.

## Claims

1. A device for sealing an opening in an anatomical structure within a living body comprising:

a flexible tube including proximal and distal parts extending along an axis wherein the proximal and distal parts are coupled together by a central part which extends away from the axis to form a gap between a distal end of the proximal part and a proximal end of the distal part and wherein the proximal part includes an end portion which, when the device is in an operative position, is located outside the body; at least one needle retention channel formed within the distal part for holding a plurality of

needles therein, wherein the needle retention channel extends along the axis to an opening formed in the proximal end of the distal part; a needle receiving channel formed within the proximal part and extending along the axis to an opening formed in the distal end of the proximal part; and a lumen extending from an opening formed in the first end of the proximal part to the needle retention channel;

wherein, when the device is in an operative position, the flexible tube extends through the opening in the anatomical structure with the opening in the distal end of the proximal part and the opening in the proximal part on opposite sides of the anatomical structure.

2. A device according to claim 1, further including a suture removal slot which communicates with the needle receiving channel to open the needle receiving channel to the outside of the flexible tube.
3. A device according to claim 1, wherein the flexible tube is circular in cross-section and includes two needle retention channels arranged side-by-side.
4. A device according to claim 1, wherein the flexible tube is oval in cross-section and includes four needle retention channels arranged side-by-side.
5. A device according to claim 1, wherein the flexible tube is formed of a first plastic piece including the proximal and central portions, coupled to a second piece comprising the distal part.
6. A device according to claim 1, wherein the lumen has a circular cross-section.
7. A device according to claim 1, wherein the lumen has a plurality of channels arranged side-by-side and wherein the cross-section of each of the side-by-side channels is semi-circular.
8. A device according to claim 1, wherein the needle retention channel includes a first substantially circular portion sized to accommodate a needle and a second portion, coupled to the first portion, wherein the second portion is sized to prevent entry of the needle therein.
9. A device according to claim 1, further including a guide wire lumen extending through the distal part.
10. A device according to claim 1, wherein the distal part is formed of a material having an increased flexibility relative to the central and proximal parts.
11. A device according to claim 1, wherein a distal end

of the distal part is biased so that, in an unstressed state, the distal part is substantially "J-shaped" with the distal end curved away from the axis.

12. A device according to claim 1, further including a substantially straight stiffening member which, when inserted into the lumen, straightens the central part so that the entire device extends substantially along the axis.
13. A device according to claim 1, further including a stiffening member including a curved central portion, wherein the flexible tube, in an unstressed state is substantially straight and, when the stiffening member is in a desired position within the lumen, is bent to form the curved central part of the device.
14. A surgical stitching device Comprising:  
a flexible tube including a substantially linear proximal part defining an axis and a substantially linear distal part extending along the axis and a curved central part coupling the proximal and distal parts so that a gap is formed therebetween;  
a needle retention channel extending through the distal part and extending along the axis to an opening formed in the proximal end of the distal part facing the gap, wherein the needle retention channel is sized to hold a plurality of needles side-by-side therein; and  
a needle receiving channel extending through the proximal part along the axis to an opening formed in the distal end of the proximal part.
15. A device according to claim 14, wherein the flexible tube is formed of a first molded part and a second extruded part bonded together.
16. A surgical stitching device comprising:  
a flexible tube including substantially linear proximal and distal parts defining an axis and a curved central part coupling the proximal and distal parts so that a gap is formed therebetween;  
a puncture needle channel extending through the proximal part along the axis to an opening formed in the distal end of the proximal part;  
a puncture needle receiving channel extending through the distal part along the axis to a suture retention channel, wherein the cross-sectional area of the suture retention channel is greater than the cross-sectional area of the puncture needle receiving channel;  
a puncture needle including a central lumen, the puncture needle being slidably received in the puncture needle channel so that, by apply-

ing pressure to a proximal end of the puncture needle, a user may manually move the puncture needle out of the opening formed in the distal end of the puncture needle channel, across the gap and into the puncture needle retention channel so that a distal end of the puncture needle is received within the suture retention chamber; and

a piston slidably received in the central lumen so that, when the distal end of the puncture needle is received within the suture retention chamber, a user may move the piston distally through the central lumen.

17. A surgical stitching device according to claim 16, wherein the flexible tube is formed of a first plastic piece including the proximal and central portions, coupled to a second piece comprising the distal part.
18. A surgical stitching device according to claim 16, wherein the puncture needle channel is substantially circular in cross-section and includes a slot which opens the channel to the outside of the flexible tube.
19. A surgical stitching device according to claim 16, wherein the puncture needle includes a radially protruding proximal end and a sharpened distal end.
20. A surgical stitching device according to claim 16, wherein a distal end of the piston includes gripping means for selectively gripping structures received in the suture retention chamber.



FIG. 3A

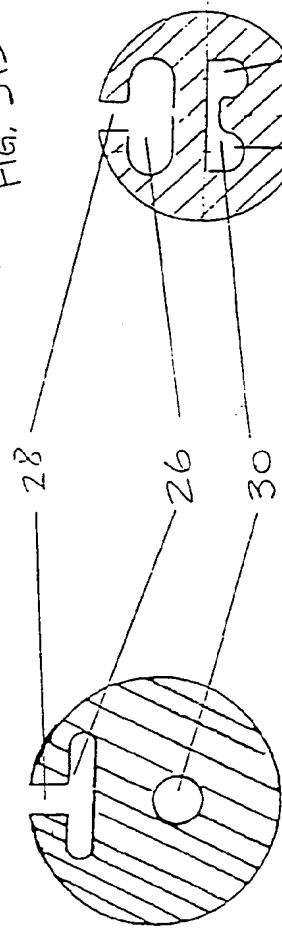


FIG. 3B

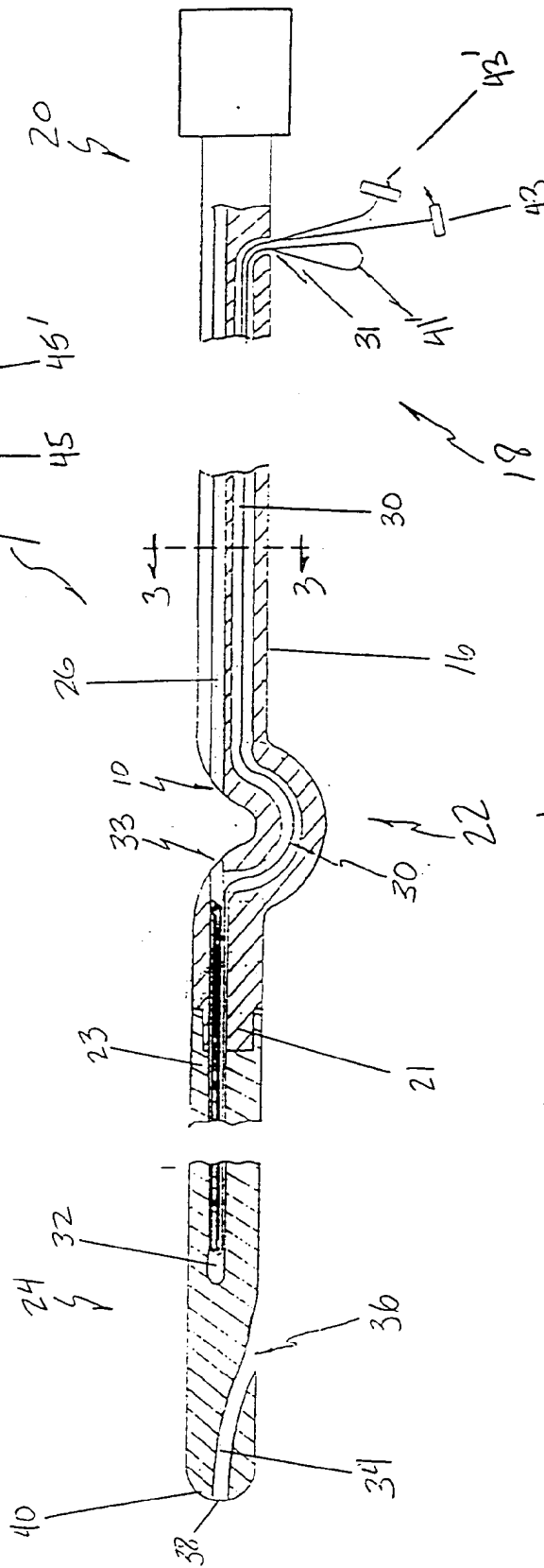
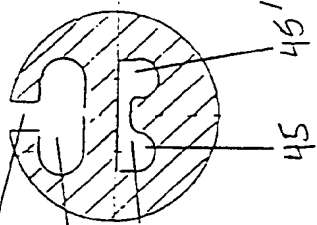
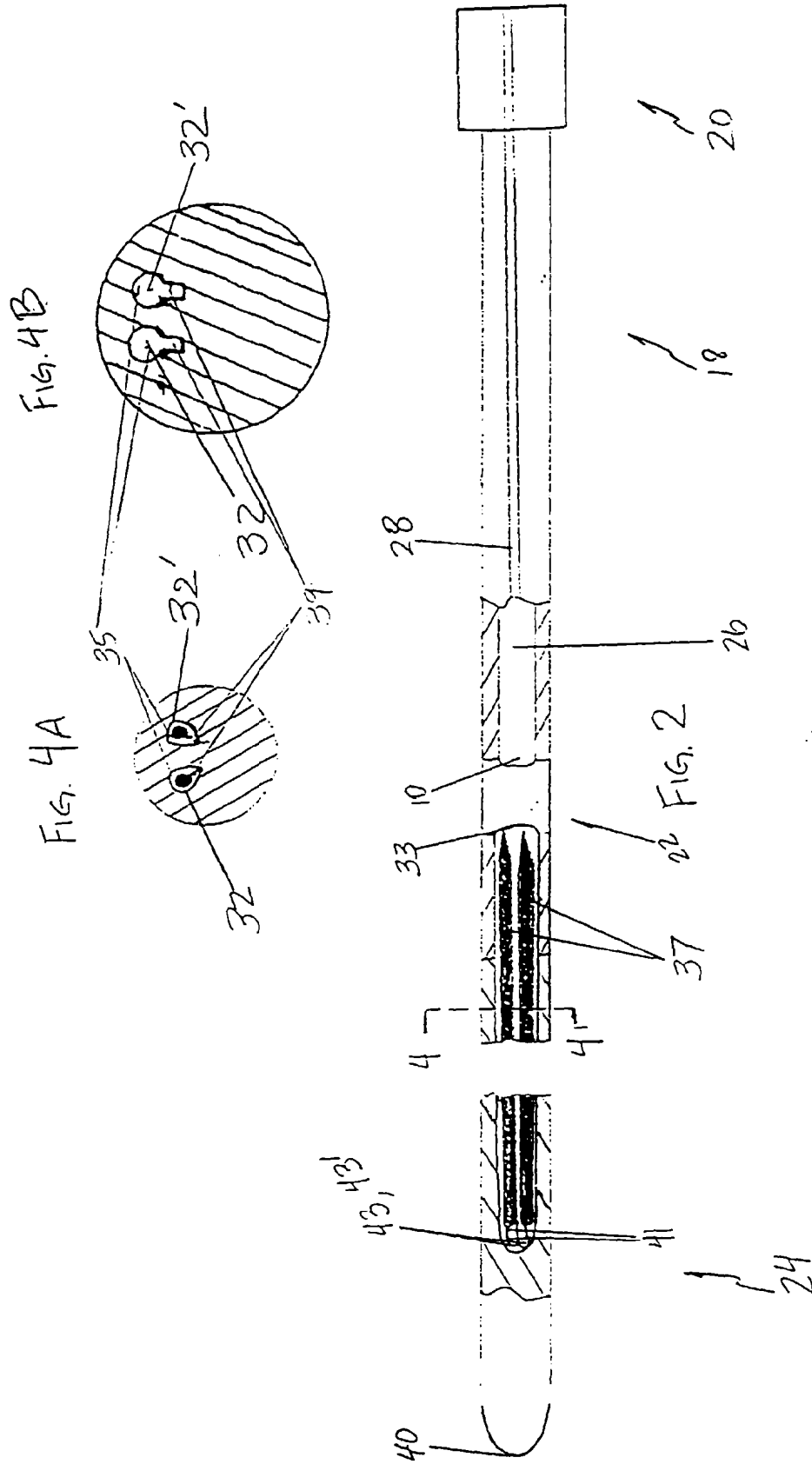
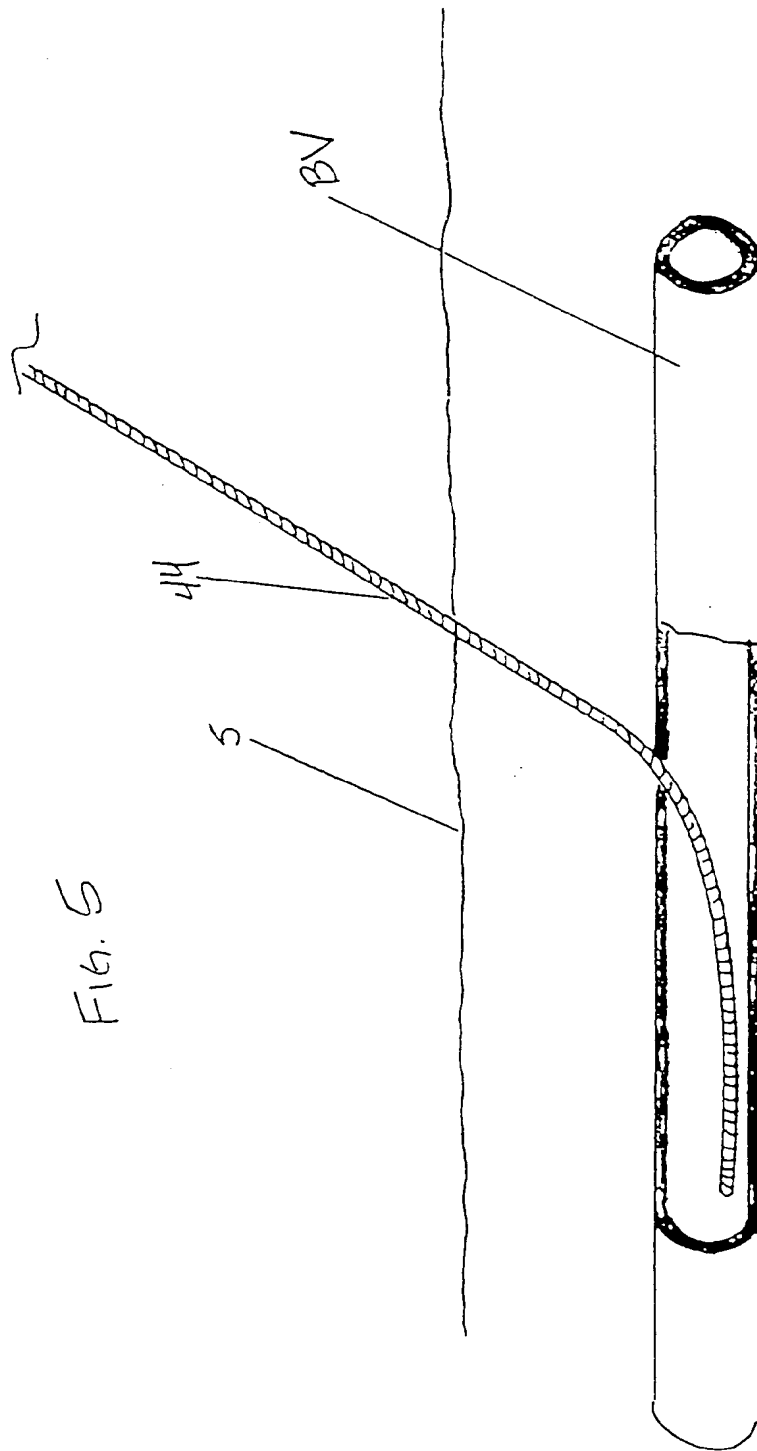
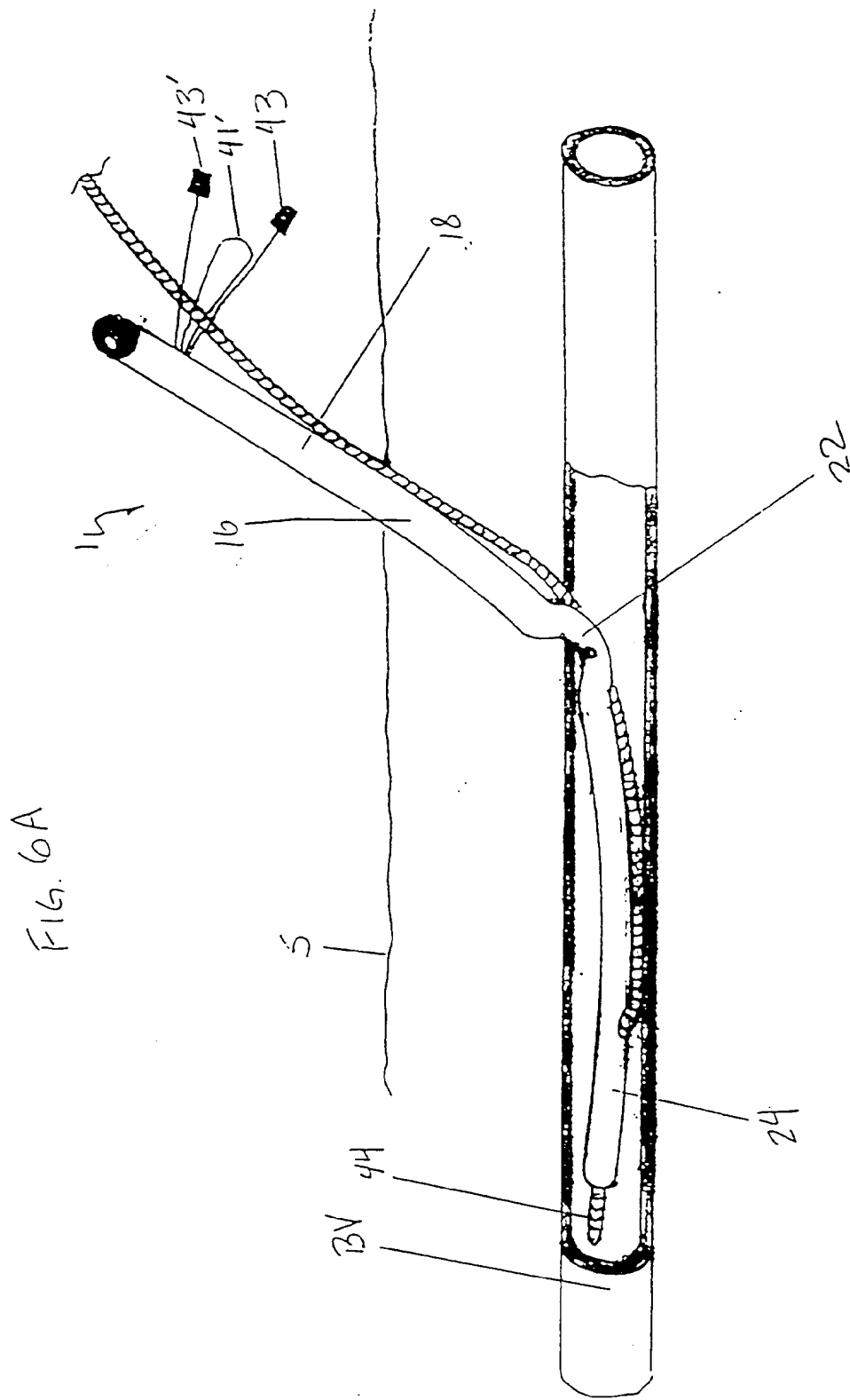
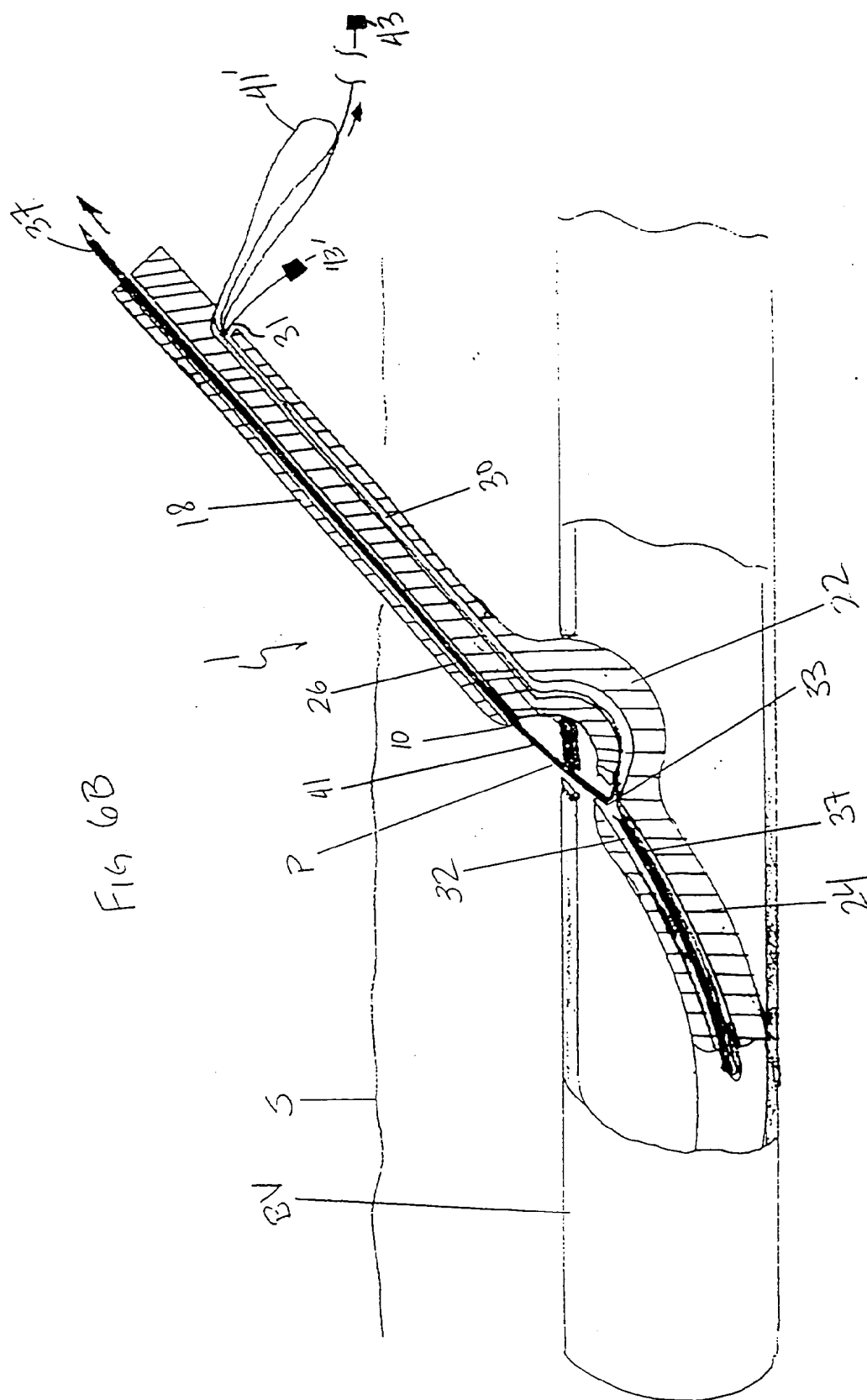


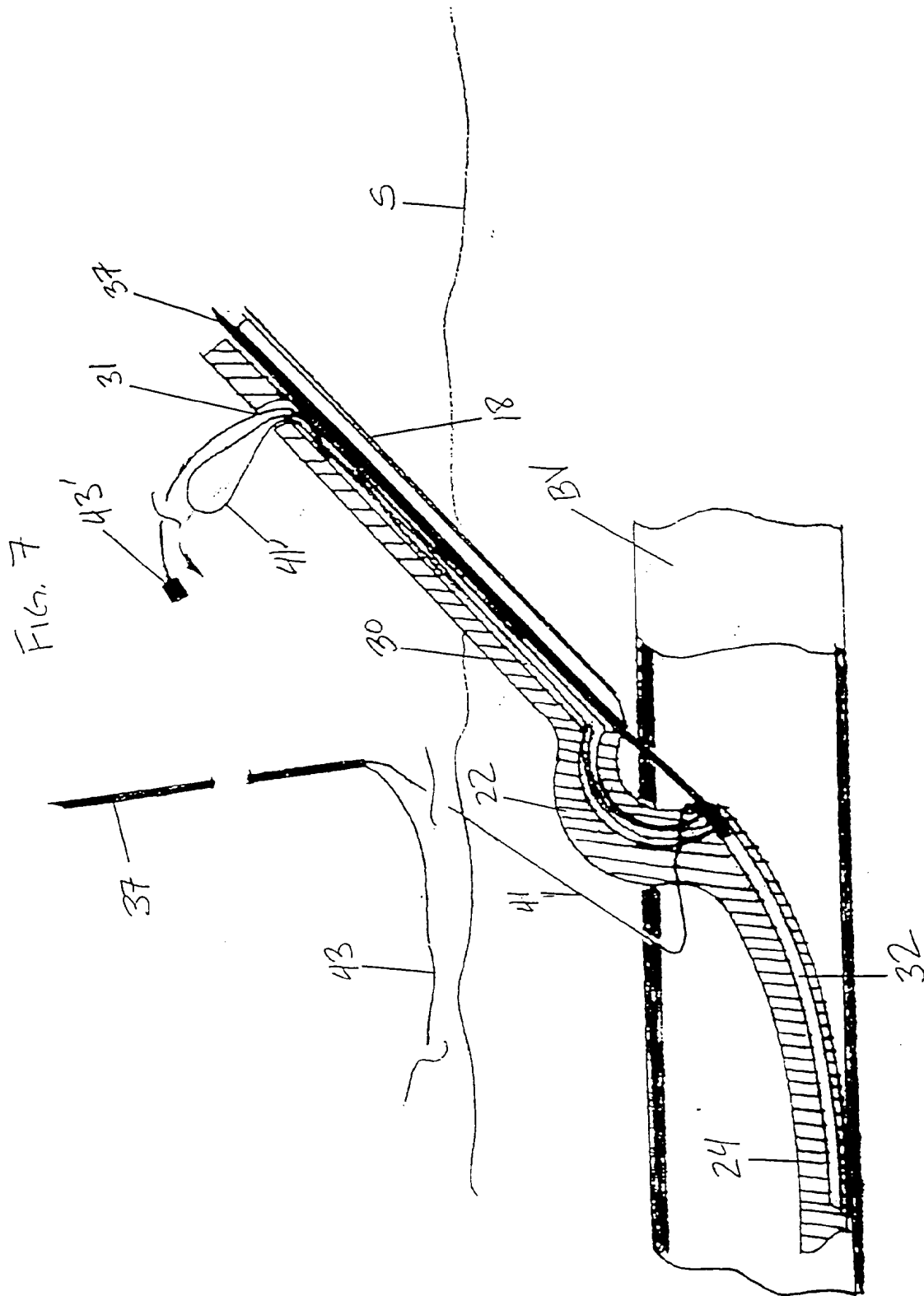
FIG. 1

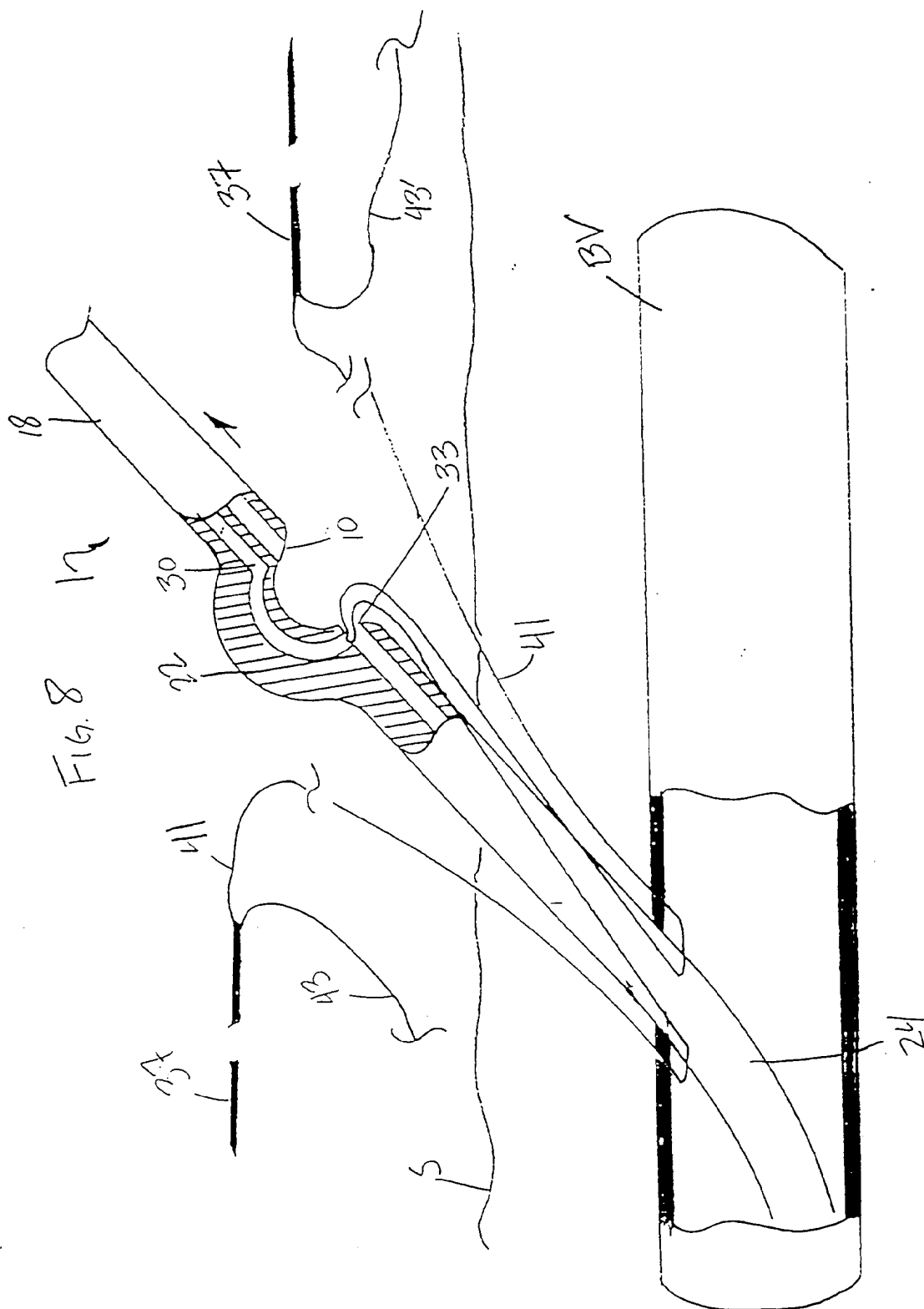


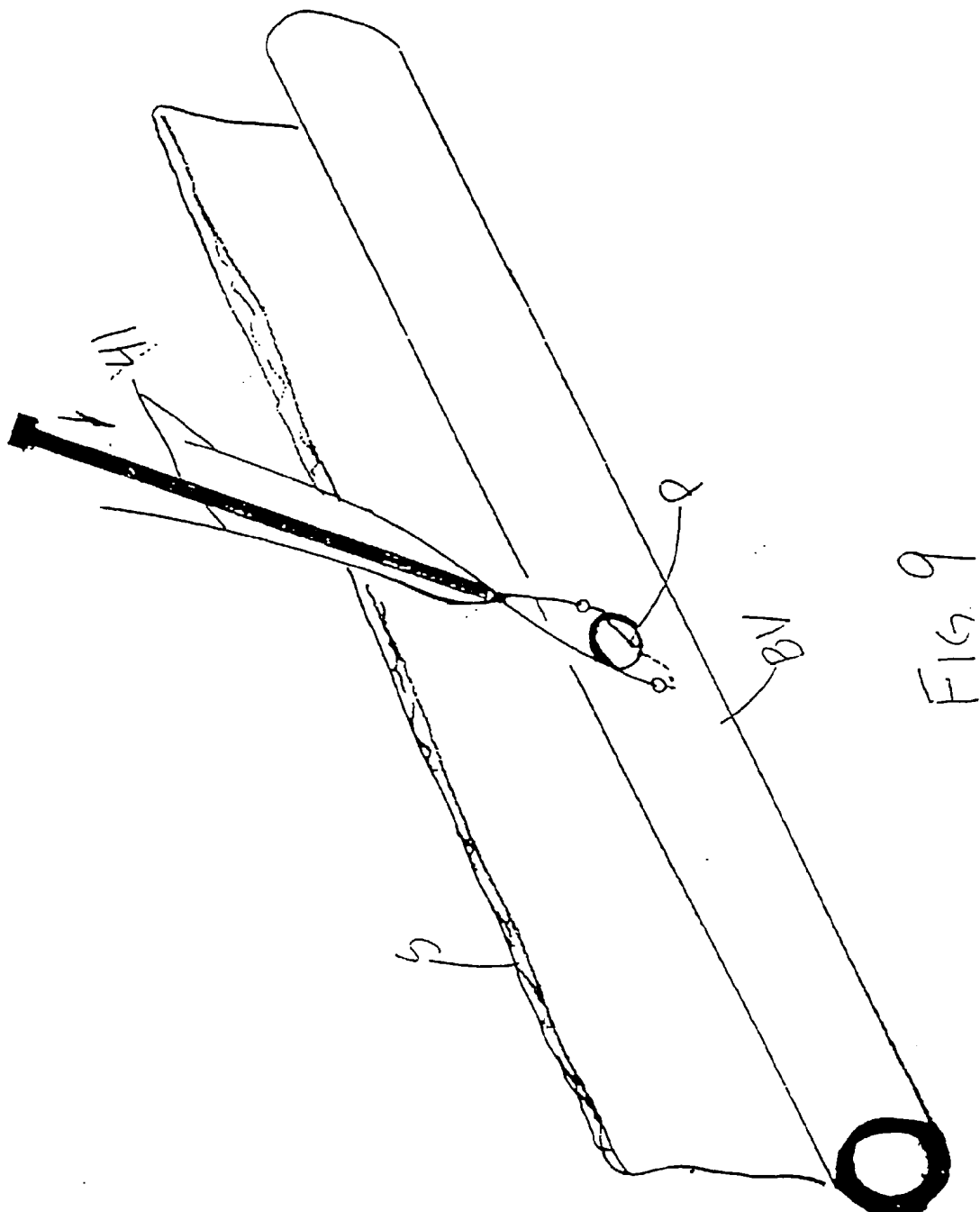














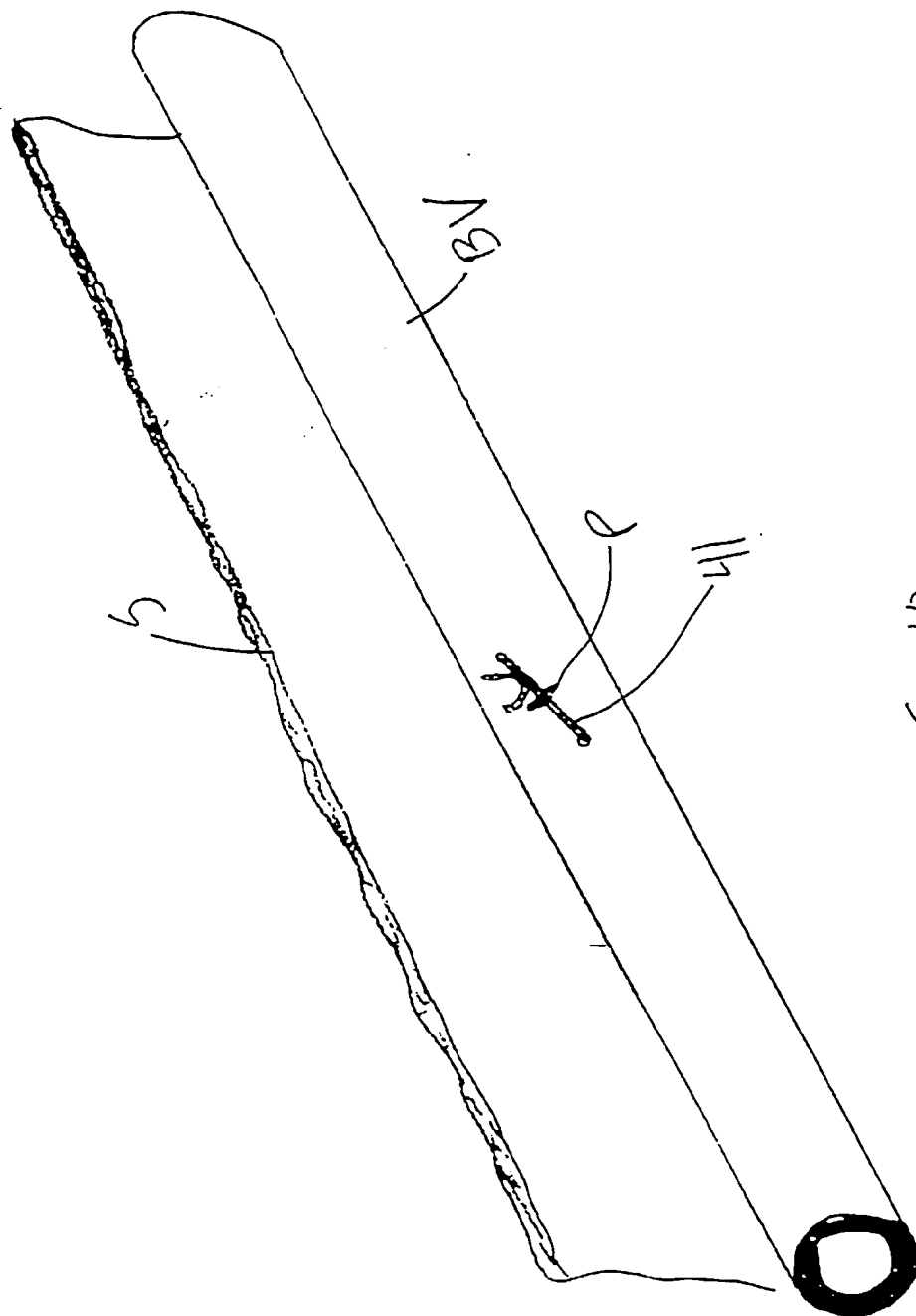
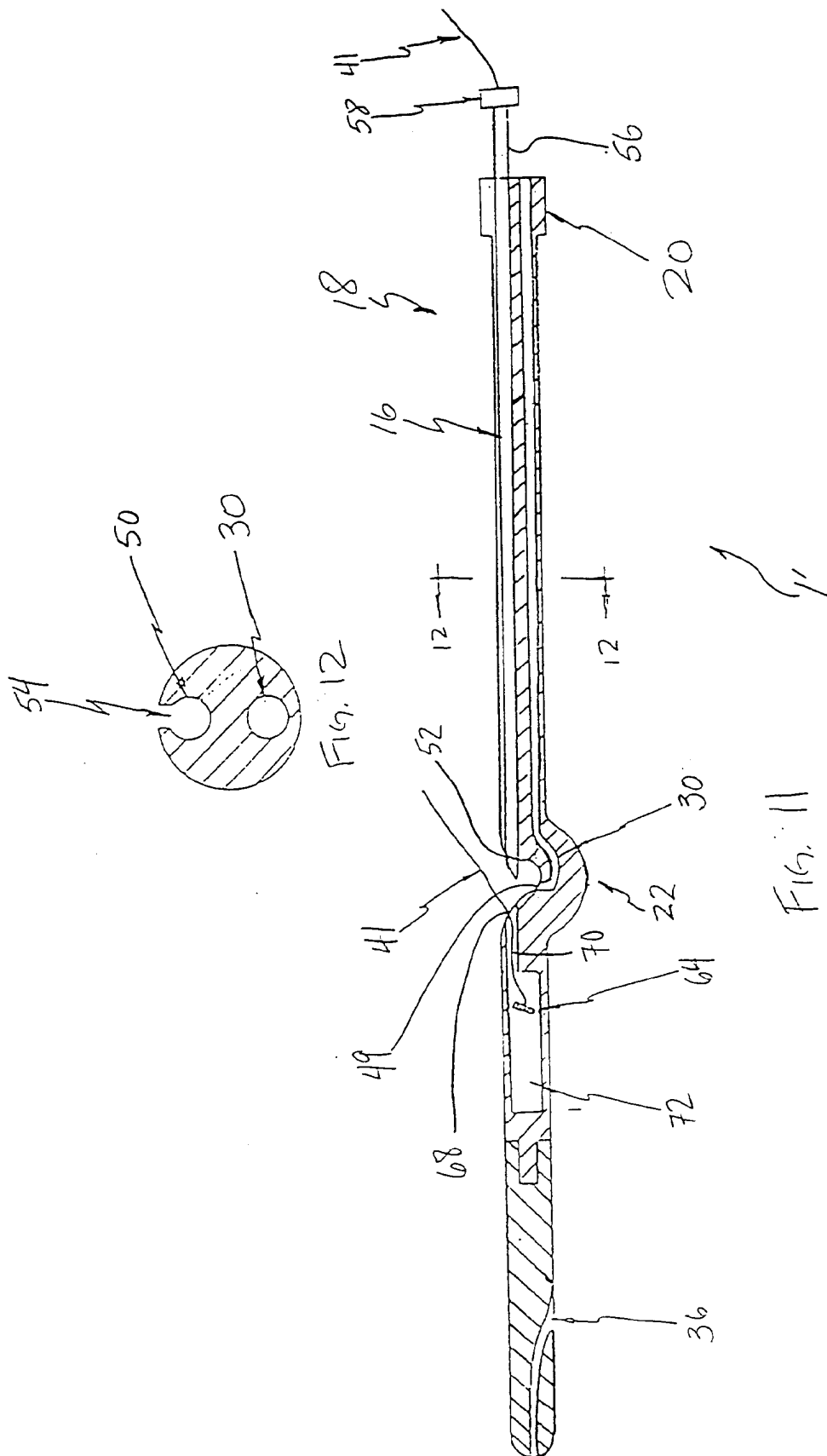


Fig. 10



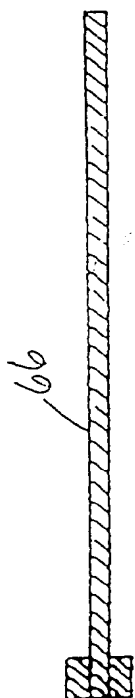


Fig. 14

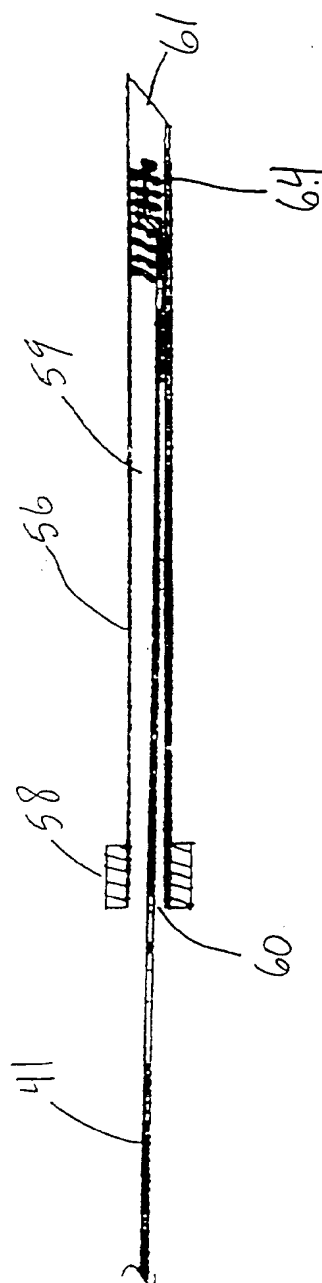
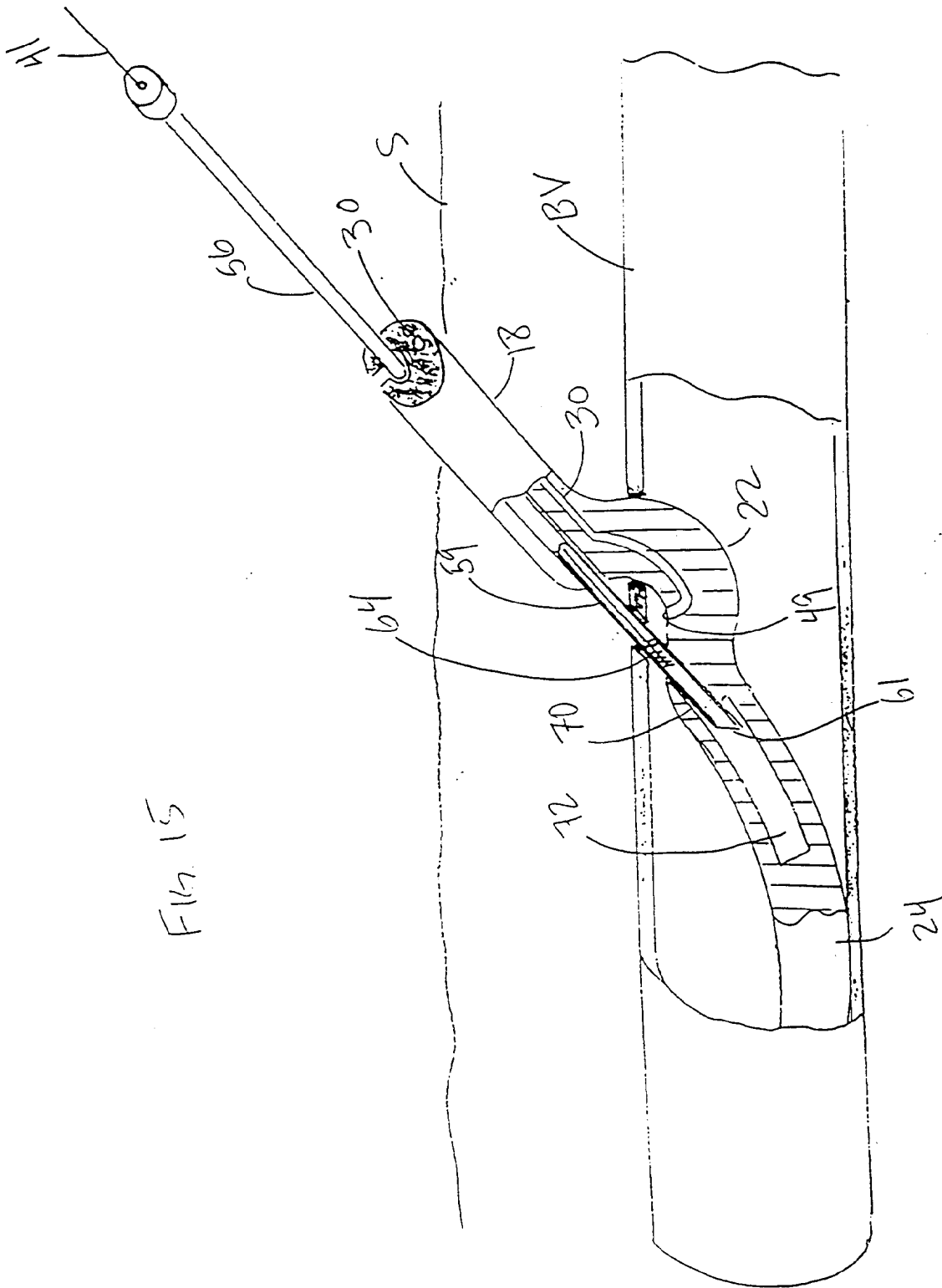
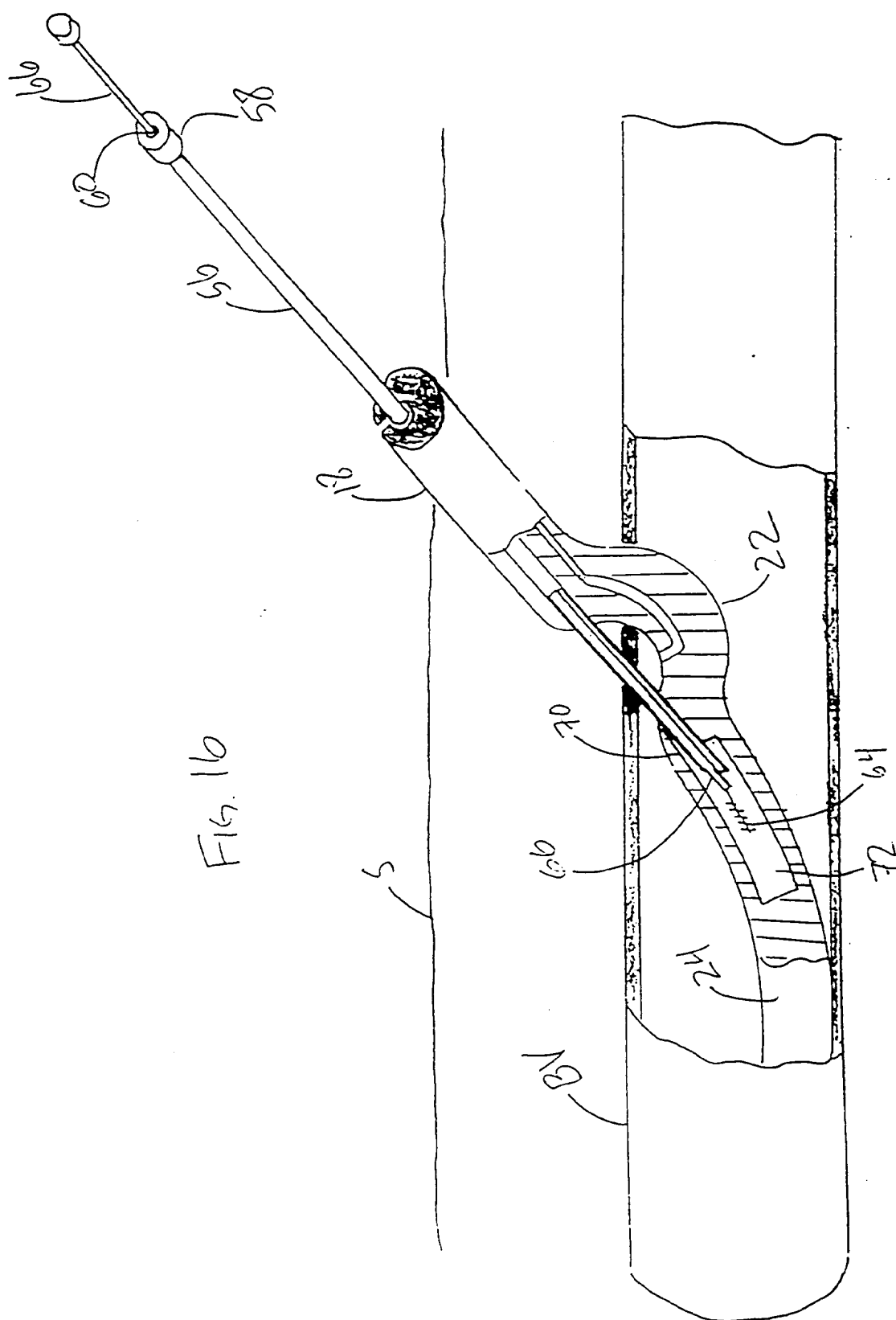
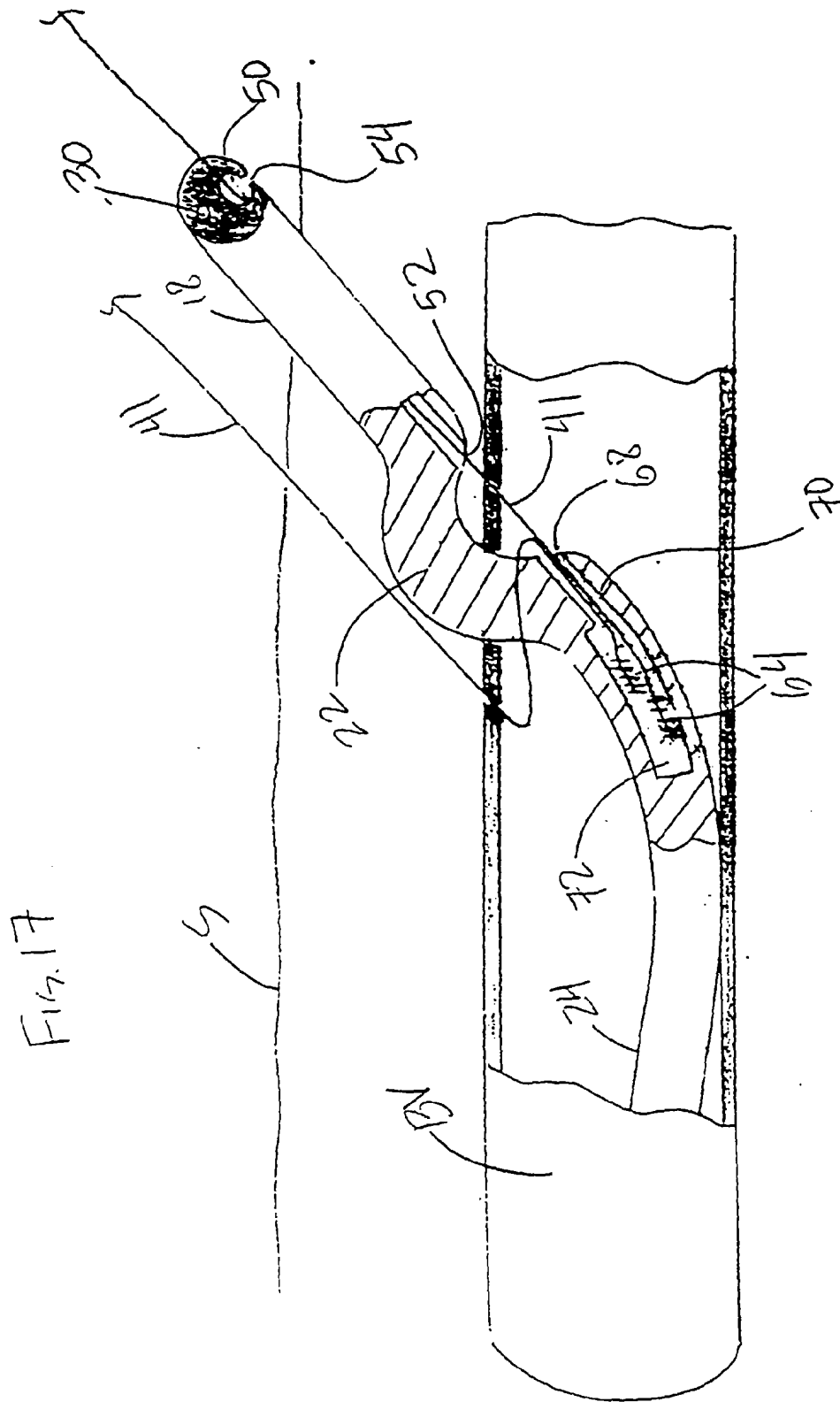


Fig. 13







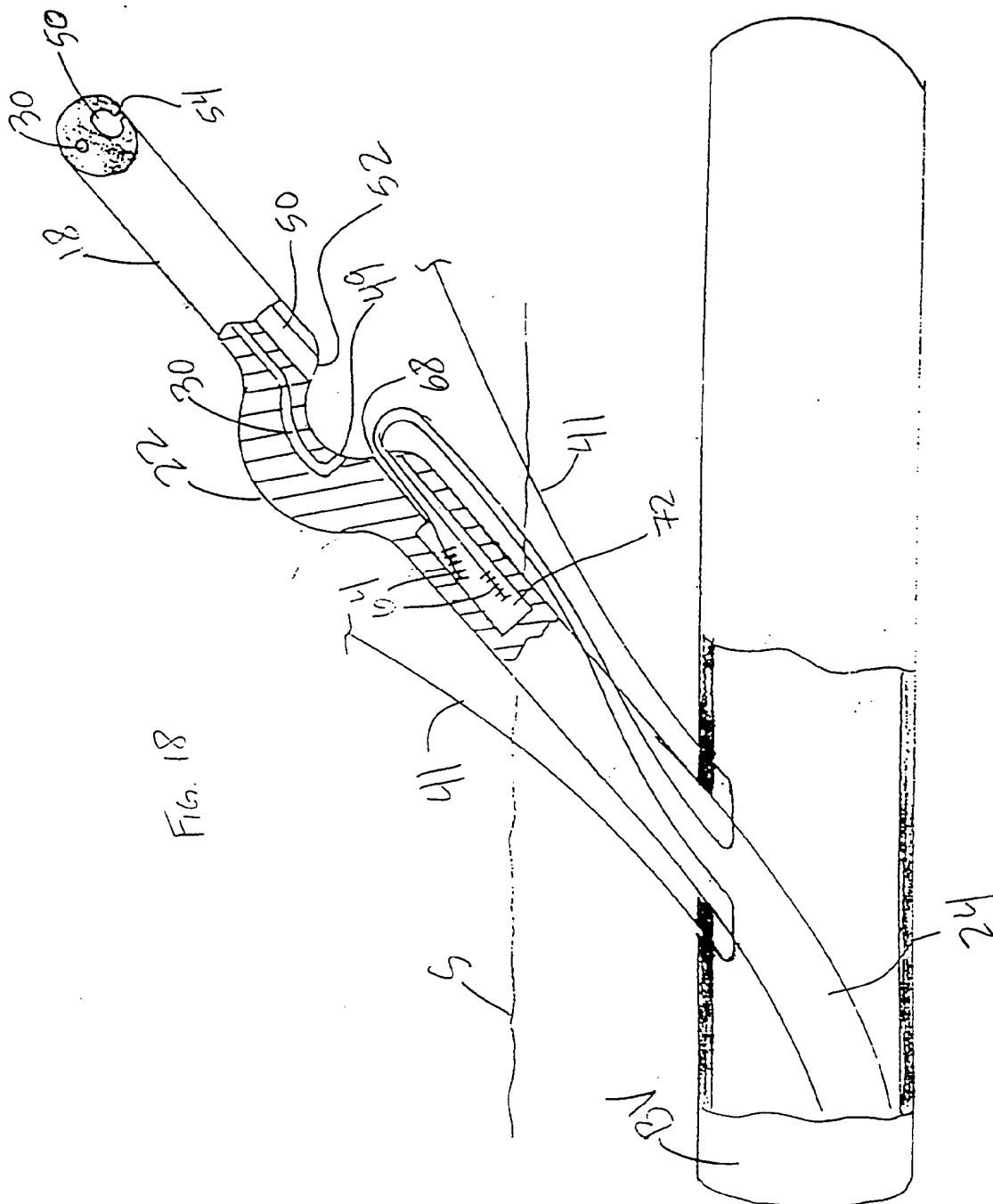


Fig. 18

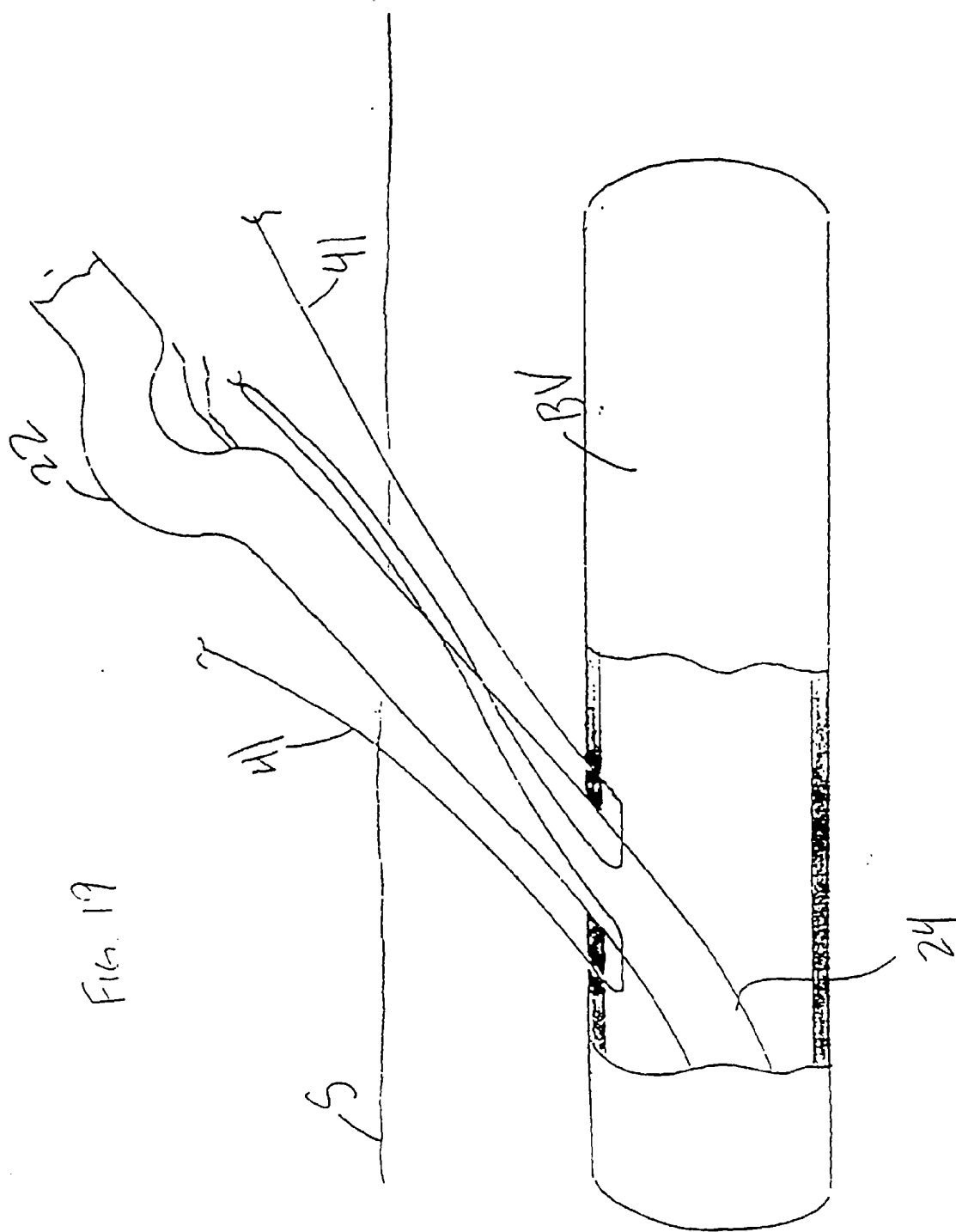
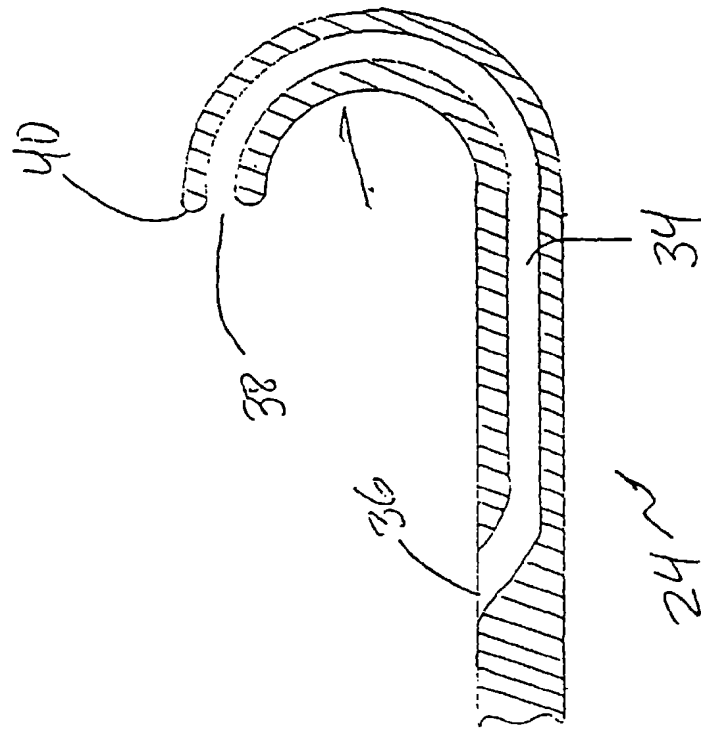
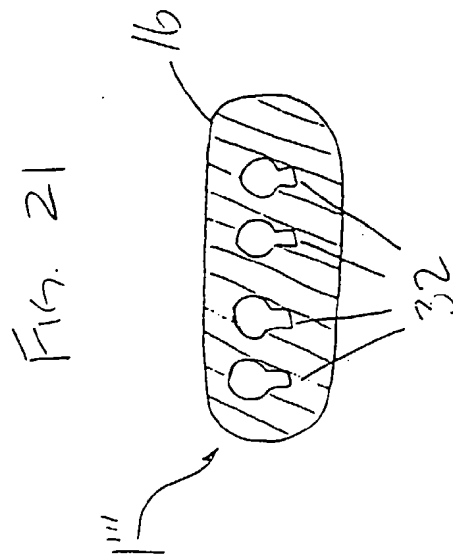




Fig 20







European Patent  
Office

# EUROPEAN SEARCH REPORT

Application Number  
EP 97 30 1486

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.6)
D,A	US 5 417 699 A (KLEIN ENRIQUE J ET AL) 23 May 1995 * the whole document *	1,14,16	A61B17/00 A61B17/04
A	WO 95 13021 A (PERCLOSE INC) 18 May 1995 * abstract; figure 1 *	1,14,16	
A	US 5 304 184 A (HATHAWAY DAVID ET AL) 19 April 1994 * abstract; figures 3,25 *	1,14,16	
A	EP 0 637 431 A (VODA JAN) 8 February 1995 * abstract; figures 9,15A *	1,14,16	
			TECHNICAL FIELDS SEARCHED (Int.Cl.6)
			A61B
The present search report has been drawn up for all claims			
Place of search		Date of completion of the search	Examiner
BERLIN		12 September 1997	Jameson, P
<p><b>CATEGORY OF CITED DOCUMENTS</b></p> <p>X : particularly relevant if taken alone  Y : particularly relevant if combined with another document of the same category  A : technological background  O : non-written disclosure  P : intermediate document</p> <p>T : theory or principle underlying the invention  E : earlier patent document, but published on, or after the filing date  D : document cited in the application  L : document cited for other reasons  &amp; : member of the same patent family, corresponding document</p>			

EPO FORM 1503 03.82 (P04C01)